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Abstract—We propose an ultrasound speckle filtering method for not only preserving various edge features but also filtering tissue-dependent complex speckle noises in ultrasound images. The key idea is to detect these various edges using a phase congruence-based edge significance measure called phase asymmetry (PAS), which is invariant to the intensity amplitude of edges and takes 0 in non-edge smooth regions and 1 at the idea step edge, while also taking intermediate values at slowly varying ramp edges. By leveraging the PAS metric in designing weighting coefficients to maintain a balance between fractional-order anisotropic diffusion and total variation (TV) filters in TV cost function, we propose a new fractional TV framework to not only achieve the best despeckling performance with ramp edge preservation but also reduce the staircase effect produced by integral-order filters. Then, we exploit the PAS metric in designing a new fractional-order diffusion coefficient to properly preserve low-contrast edges in diffusion filtering. Finally, different from fixed fractional-order diffusion filters, an adaptive fractional order is introduced based on the PAS metric to enhance various weak edges in the spatially transitional areas between objects. The proposed fractional TV model is minimized using the gradient descent method to obtain the final denoised image. The experimental results and real application of ultrasound breast image segmentation show that the proposed method outperforms other state-of-the-art ultrasound despeckling filters for both speckle reduction and feature preservation in terms of visual evaluation and quantitative indices. The best scores on feature similarity indices have achieved 0.867, 0.844 and 0.834 under three different levels of noise, while the best breast ultrasound segmentation accuracy in terms of the mean and median dice similarity coefficient are 96.25% and 96.15%, respectively.

Index Terms—Ultrasound despeckling, speckle noise, fractional-order diffusion filter, fractional-order TV filter, edge detection, phase congruency, phase asymmetry, image denoising.

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I. INTRODUCTION
CURRENT [1], [2] [3], [4] [5], [6] [7]. F [5] [7]. S [8], [9] [10]. T 3D 2D [11]. T [13], [14] (NLM) F [14]

[15], C *et al.* [16], M, (SBF) [17], H, T, NLM, NLM, C *et al.* [18], BNLNLM (OBNLM), Z *et al.* [19], R, Z *et al.* [20], (NLLRF), H, NLM, [21], I, P, M, (AD), [22], (SRAD) [23], (DPAD) [24], T, SRAD, DPAD, T, [25], U, C *et al.* [16], U, [26], H, [27], M, T, B, F [28], AD (FAD), N, F *et al.* [8], (ADLG), H, ADLG, AD, B, AD,

[29], [30], AD, H, E, T, A, [31], T, T, [32], O *et al.* [33], H, [2], C *et al.* [34], S, [35], [36], [37], [38], H, T, [39], [40], I, M, M *et al.* [41], [42], T, F, A, T, M, T, M, -P, N [43], W, [44], (PC)-, (PAS, (PS), T, I)

TABLE I
ACRONYMS

Acronym Description

[Redacted text block]

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(AM-FM) [48] [50] [51], [52]. T [53]

2D f R T f_M
 $f_M = (f, f_R) = (f, r_1 * f, r_2 * f)$, f_R
 $f, r_1(x_1, x_2), r_2(x_1, x_2)$
 R R, ∇ ∇ :

$$r_1(x_1, x_2) = \frac{-x_1}{2\pi(x_1^2 + x_2^2)^{3/2}}$$

$$r_2(x_1, x_2) = \frac{-x_2}{2\pi(x_1^2 + x_2^2)^{3/2}} \quad (1)$$

S f_M b. T
 $f_M = (b * f, b * r_1 * f, b * r_2 * f) =$
 $(e_s, o_s), \nabla e_s, o_s$
 S $e_s, o_s; \nabla C$
 C F [54]. I
 2D C
 ∇ :

$$C(w) = n_c |w|^a \quad (-s |w|), a \geq 1 \quad (2)$$

$w = (w_1, w_2)$, s
 $n_c = \left(\frac{\pi 4^{a+1} s^{2a+1}}{\Gamma(2a+1)}\right)^{\frac{1}{2}}, \Gamma(\cdot)$
 $a = 1.58$, [39].
 T PAS, K [44]

$$PA = \sum_s \frac{[|o_s| - |e_s| - T_s]}{\sqrt{e_s^2 + o_s^2 + \varepsilon}} \quad (3)$$

PA PAS, ε , T_s
 $[\cdot]$ C S, s
 (\cdot)

F . 1 PAS
 W PAS $s = 5, s = 10$
 $s = 25$, PAS $s = 20$
 T PAS $s = 15$
 $s = 15$

F . 1. E PAS () T
 ; PAS : () $s = 5$, () $s = 10$, () $s = 15$,
 () $s = 20$, () $s = 25$.

PAS T PAS 0 1, 0
 ()
 1 ()
 . I, PAS
 . A, PAS
 . D PAS
 . F PAS 1.

B. Fractional-Order Differential

T -
 [47]. F $f(x) \in L^2(R)$,
 ∇ :

$$D^\alpha f(x) = \frac{d^\alpha f(x)}{dx^\alpha} \quad (4)$$

$\nabla \alpha$ T F
 $D^\alpha f(x) \nabla$:

$$D^\alpha f(x) \stackrel{FT}{\Leftrightarrow} (\hat{D}^\alpha f)(w) = (iw)^\alpha \hat{f}(w)$$

$$= |w|^\alpha [i \theta^\alpha(w)] \hat{f}(w)$$

$$= |w|^\alpha \left[\frac{\alpha \pi i}{2} (w) \right] \hat{f}(w) \quad (5)$$

w ()
 $(iw)^\alpha = |w|^\alpha \left[\frac{\alpha \pi i}{2} (w) \right]$. A
 ∇
 α , F . 2. F F . 2,
 $\nabla 0 < w < 1$,
 $w > 1$,
 $\nabla \alpha$ T

D . A

F . 2. T
 [47]. E
 [46]. T
 S . III-A
 C
 (G-L) R -L (R-L) [55], [56].
 S G-L
 G-L
 [57], α -
 G-L

$$D^\alpha f(x) \triangleq \lim_{h \rightarrow 0} \frac{1}{h^\alpha} \sum_{l=0}^{\lfloor \frac{d-c}{h} \rfloor} (-1)^l \binom{\alpha}{l} f(x - lh) \quad (6)$$

α , $[c, d]$
 $\frac{d-c}{h}$, $\lfloor \frac{d-c}{h} \rfloor$, $\binom{\alpha}{l}$
 :

$$\binom{\alpha}{l} = \frac{\Gamma(\alpha + 1)}{\Gamma(l + 1)\Gamma(\alpha - l + 1)} \quad (7)$$

$\Gamma(n) = (n - 1)!$

C. Fractional-Order AD Filter and Fractional-Order TV Filter

T
 AD [22] :

$$\frac{\partial u}{\partial t} = \text{div} [c(|\nabla u|) \cdot \nabla u], \quad (8)$$

$\text{div} \nabla u$, $c(\cdot)$, $|\nabla u|$, λ , Φ , Δ , Γ

$$\Phi'(0) = 0. \quad (20)$$

$$\nabla_x^\alpha u \nabla_x^\alpha \eta + \nabla_y^\alpha u \nabla_y^\alpha \eta = \left((\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u \right) \eta \quad (21)$$

Algorithm 1 PFDTV F -P D F

Input:

$$\Phi'(0) = \varphi \int_{\Omega} c (|\nabla^\alpha u|^2, PA^2) \left((\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u \right) \eta \, dy$$

$$+ \gamma \int_{\Omega} \frac{(\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u}{|\nabla^\alpha u|} \eta \, dy$$

$$+ \lambda \int_{\Omega} (u - u_0) \eta \, dy \quad (22)$$

$\eta \in C^\infty(\Omega)$, $E = -L u$:

$$\varphi c (|\nabla^\alpha u|^2, PA^2) \left((\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u \right) + \gamma \frac{(\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u}{|\nabla^\alpha u|} + \lambda (u - u_0) = 0 \quad (23)$$

$L \nabla E$ $E(u)$; $E(u)$

$$\nabla E = \varphi c (|\nabla^\alpha u|^2, PA^2) \left((\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u \right) + \gamma \frac{(\nabla_x^\alpha)^* \nabla_x^\alpha u + (\nabla_y^\alpha)^* \nabla_y^\alpha u}{|\nabla^\alpha u|} + \lambda (u - u_0) \quad (24)$$

Δt u $-\nabla E, i.e., u^{n+1} = u^n + \Delta t(-\nabla E)$. F $E(u)$.

C. Numerical Algorithm

Δt u $G-L$ u $X \times Y$ X Y

$\nabla_x^\alpha, \nabla_y^\alpha, (\nabla_x^\alpha)^*, (\nabla_y^\alpha)^*$:

$$\begin{cases} \nabla_x^\alpha u_{i,j} = \sum_{l=0}^j (-1)^l \binom{\alpha}{l} u_{i,j-l} \\ \nabla_y^\alpha u_{i,j} = \sum_{l=0}^i (-1)^l \binom{\alpha}{l} u_{i-l,j} \end{cases} \quad (25)$$

$$\begin{cases} (\nabla_x^\alpha)^* u_{i,j} = \sum_{l=0}^{Y-1-j} (-1)^l \binom{\alpha}{l} u_{i,j+l} \\ (\nabla_y^\alpha)^* u_{i,j} = \sum_{l=0}^{X-1-i} (-1)^l \binom{\alpha}{l} u_{i+l,j} \end{cases} \quad (26)$$

TABLE II
COMPARISON OF THE PSNR, MSSIM AND FSIM VALUES AMONG DIFFERENT FILTERS



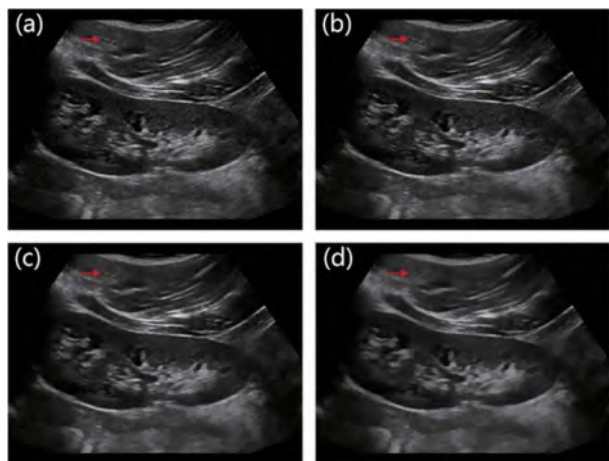
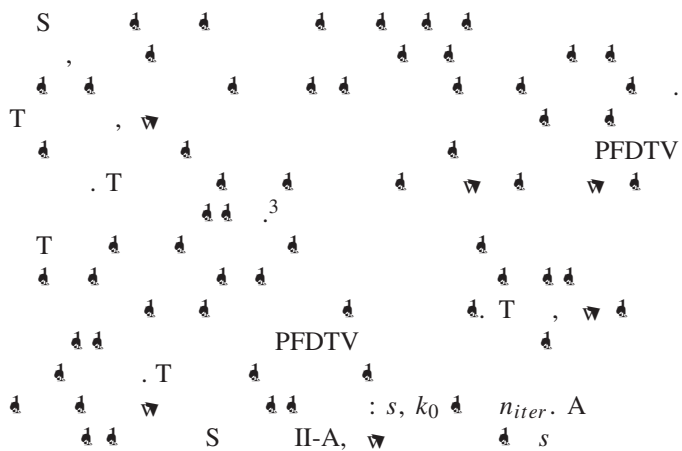


Fig. 4. Experimental results of the proposed method for different values of k_0 . (a) Original image, (b) $k_0 = 5$, (c) $k_0 = 20$, (d) $k_0 = 100$.



B. Clinical Image Experiment



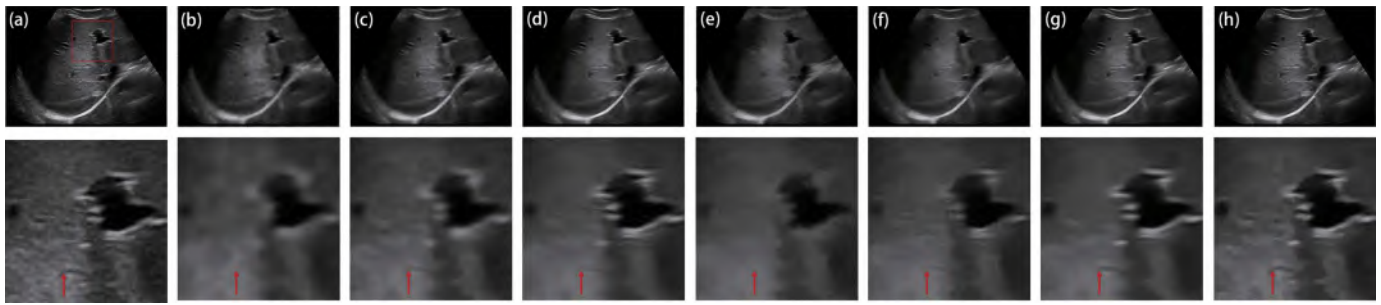


Fig. 6. Denoising results of the original image (a) using (b) SRAD, (c) OBNLM, (d) SBF, (e) ADLG, (f) NLLRF, and (g) PFDTV. The zoomed images show the results of the denoising process on the regions of interest (ROI) marked by the red arrows in the original image (a). The zoomed images show that PFDTV (g) and SRAD (b) preserve the most detail while effectively removing noise.

Fig. 7. Denoising results of the original image (a) using (b) OBNLM, (c) SBF, (d) ADLG, (e) NLLRF, and (f) PFDTV. The zoomed images show the results of the denoising process on the regions of interest (ROI) marked by the red arrows in the original image (a). The zoomed images show that PFDTV (f) and SRAD (b) preserve the most detail while effectively removing noise.

SRAD, PFDTV, OBNLM, NLLRF, SBF, ADLG, and T. The zoomed images show the results of the denoising process on the regions of interest (ROI) marked by the red arrows in the original image (a). The zoomed images show that PFDTV (f) and SRAD (b) preserve the most detail while effectively removing noise.

Fig. 8. DSC, JS, HD and HM values for different segmentation methods on ten breast ultrasound images. The methods compared are: (a) T, (b) F, (c) SRAD, (d) OBNLM, (e) SBF, (f) ADLG, (g) NLLRF, and (h) PFDTV.

Table III shows the mean DSC, JS, HD and HM values for different segmentation methods on ten breast ultrasound images. The methods compared are: (a) T, (b) F, (c) SRAD, (d) OBNLM, (e) SBF, (f) ADLG, (g) NLLRF, and (h) PFDTV. The results show that PFDTV achieves the highest DSC and JS values, and the lowest HD and HM values, indicating superior segmentation performance.

TABLE III
THE MEAN DSC, JS, HD AND HM VALUES FOR DIFFERENT SEGMENTATION RESULTS ON TEN BREAST ULTRASOUND IMAGES

	DSC(%)	JS(%)	HD	HM
Input	91.87	85.02	16.9933	3.3599
Frost	93.62	88.02	9.8418	2.1265
SRAD	94.02	90.52	8.2271	1.5781

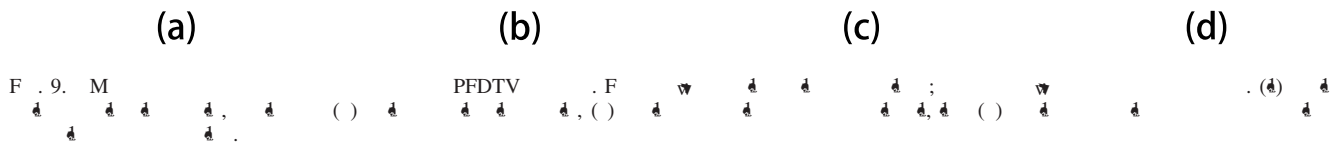


Fig. 9. Median DSC, JS, HD and HM values for different segmentation results on ten breast ultrasound images. (a) Original image, (b) SRAD, (c) OBNLM, (d) SBF, (e) ADLG, (f) NLLRF, (g) PFDTV.

TABLE IV
THE MEDIAN DSC, JS, HD AND HM VALUES FOR DIFFERENT SEGMENTATION RESULTS ON TEN BREAST ULTRASOUND IMAGES

[2], ACVA, G, P, -G, T, [78], [79],
 PFDTV, I, [35], [76], [80], M, 3D, [7], [81],
 H, W, fi, T, [82], W, T, s, [39], F, [38], [39],
 I, TV, FAD, FTV, S, TV

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T, W, W, d, d

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